

Velocity-Corrected Rectified Flow for Volumetric Cross-Modality Medical Image Synthesis

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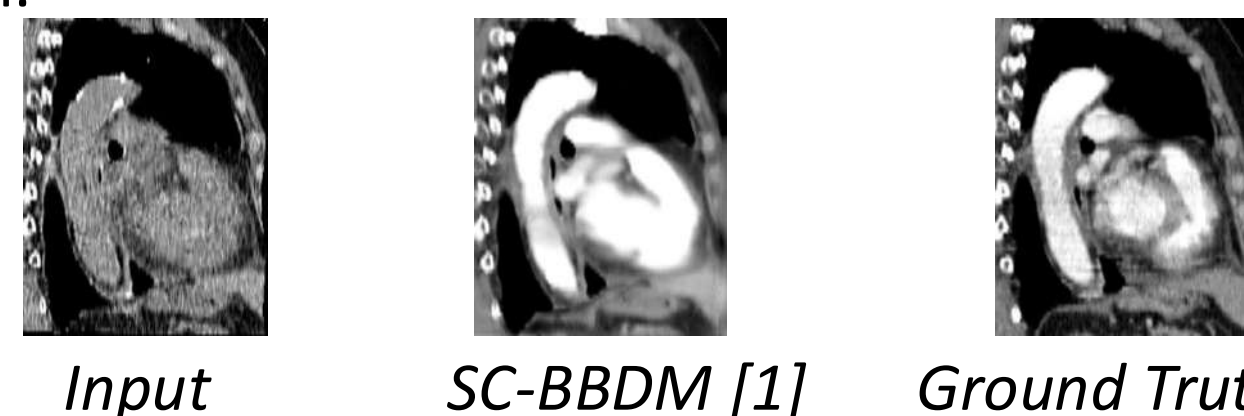
1. M.R. and P.S. contributed equally to this work.



BACKGROUND

- Contrast-enhanced CT improves visualization of vascular and soft-tissue structures, helping clinicians better identify abnormalities [1]. However, obtaining contrast-enhanced scans requires injecting contrast agents, which may not always be preferred or available.

- Diffusion models iteratively denoise images over 50–1000 steps [2], making inference slow. GANs [3] are faster but difficult to train.



- SCBBDM [1] shows promising performance but fails to adequately enhance contrast, producing oversmoothed images with loss of structural detail.

- VCRF [4] uses rectified flow to learn a deterministic neural ODE mapping in only 3 steps.

- A lightweight 2D velocity correction aggregates neighboring slices for 3D volumetric consistency, avoiding the high computational cost of full 3D models, $x_{t-1} \leftarrow x_{t-1} - \gamma_k \bar{v}_\theta$

Where \bar{v}_θ averages velocity for 3D consistency.

OBJECTIVE

To generate contrast-enhanced CT images from non-contrast images, applying velocity-corrected rectified flow for volumetric cross-modality medical image synthesis.

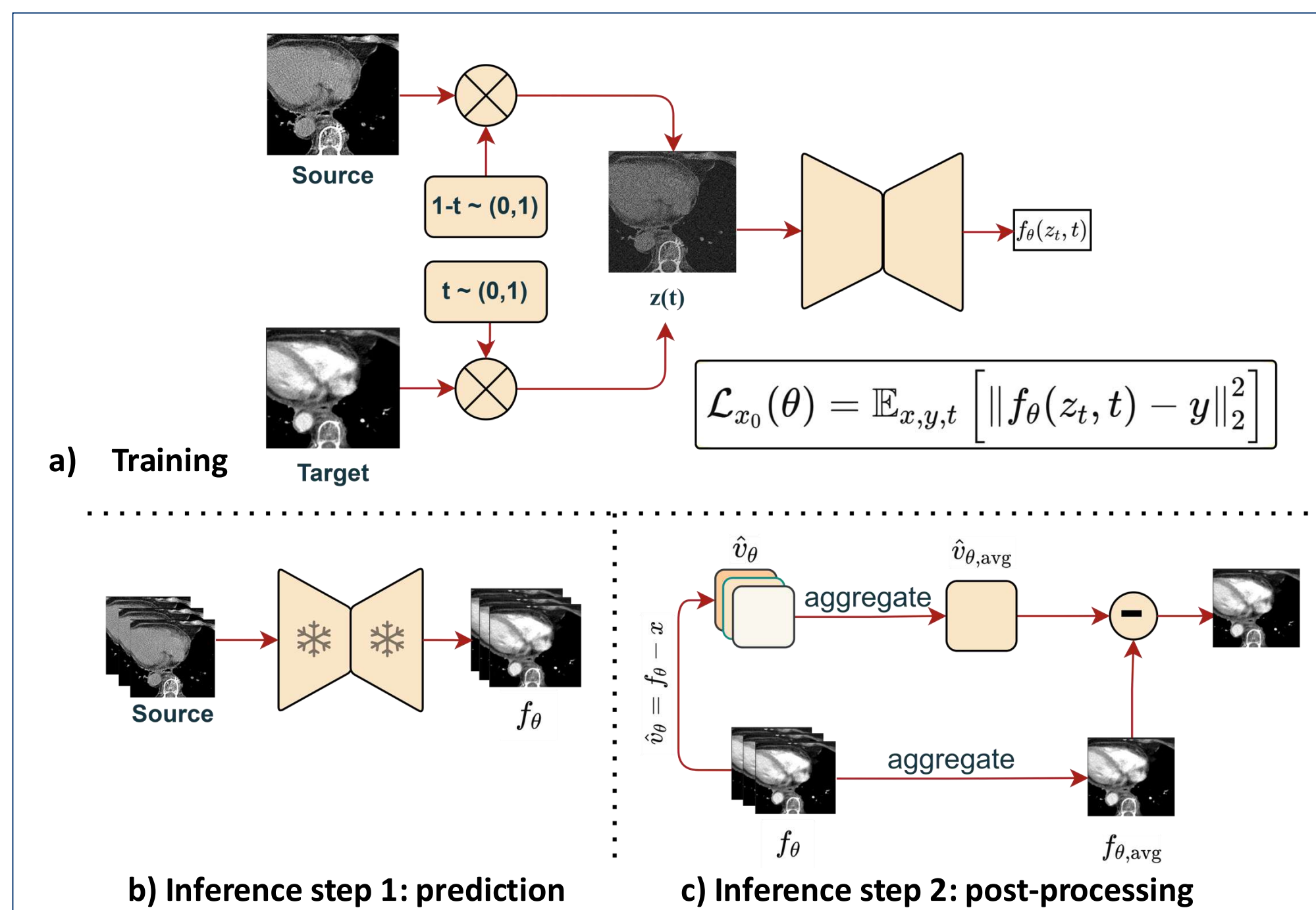
METHOD

- Linear interpolation paths: $x_t = (1 - t)x_0 + ty$, $t \in [0,1]$
- Train f_θ to predict target volume: $\mathcal{L}_{x_0} = \mathbb{E}_{x,y,t} [\|f_\theta(x_t, t) - y\|_2^2]$
- Solve ODE backward in 3 discrete steps.
- Velocity Correction

1) Recompute velocity: $\tilde{v}_\theta = \hat{v}_\theta(x_{t-1}, t - 1)$

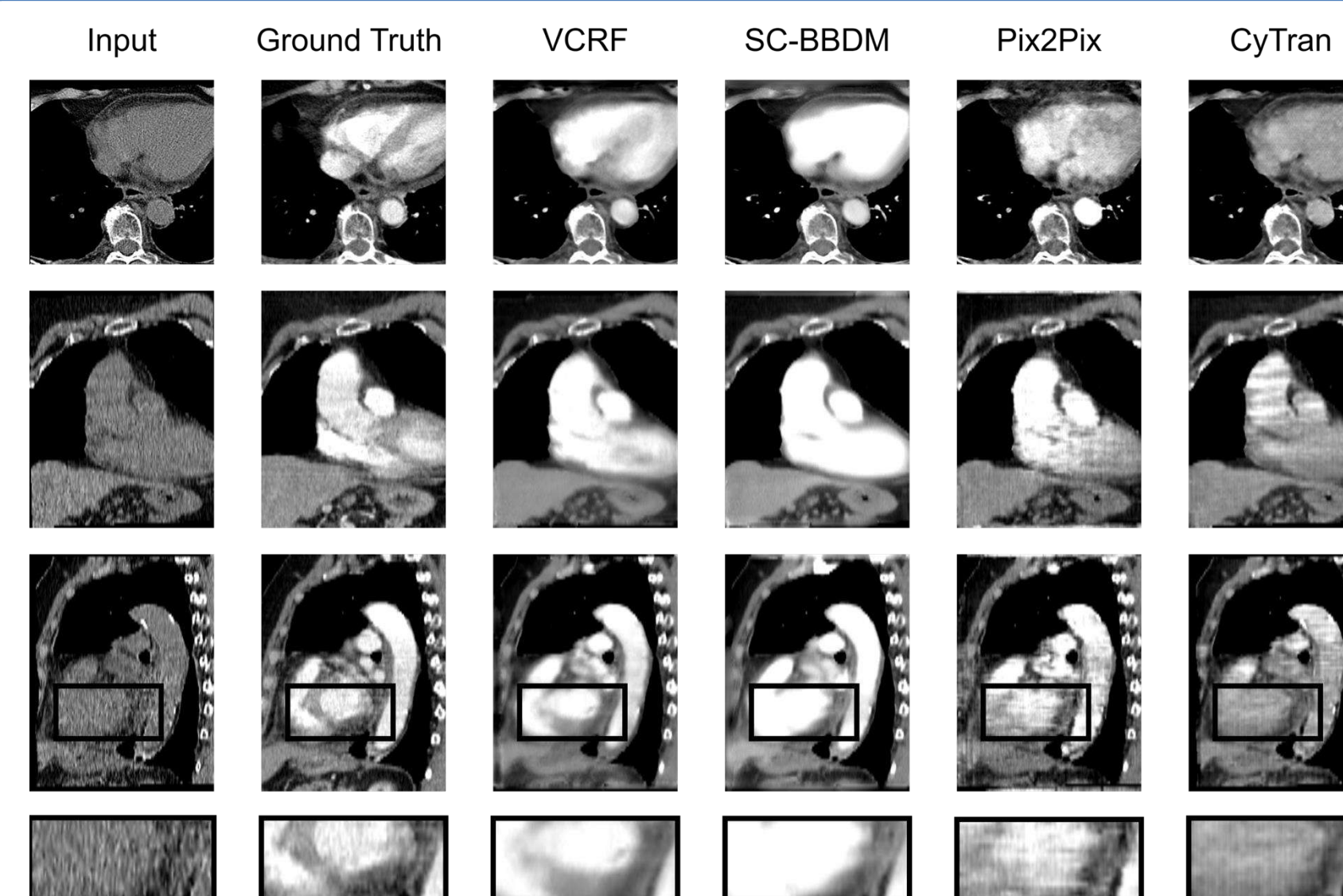
2) Aggregate neighboring slices.

3) Apply corrective update: $\gamma_k = \alpha \Delta t_k \frac{\sqrt{HW}}{\|\tilde{v}_\theta\|_2}$



Results

| Model | FID↓ | | | LPIPS _{Rad} ↓ | | | SSIM _{2D} ↑ | | | NMRSE↓ | PSNR↑ |
|---------|--------------|--------------|--------------|------------------------|-------------|-------------|----------------------|-------------|-------------|--------------|--------------|
| | AXI | COR | SAG | AXI | COR | SAG | AXI | COR | SAG | | |
| CyTran | 37.70 | 51.84 | 35.03 | 0.50 | 0.44 | 0.39 | 0.77 | 0.73 | 0.58 | 0.085 | 22.36 |
| Pix2Pix | 18.07 | 117.05 | 96.48 | 0.39 | 0.44 | 0.40 | 0.81 | 0.76 | 0.71 | 0.074 | 22.93 |
| SC-BBDM | 40.63 | 41.63 | 41.49 | 0.32 | 0.35 | 0.22 | 0.90 | 0.87 | 0.88 | 0.042 | 27.83 |
| VCRF | 32.11 | 31.85 | 32.93 | 0.29 | 0.24 | 0.21 | 0.90 | 0.88 | 0.89 | 0.037 | 29.65 |



All visualizations are displayed using the soft-tissue window setting (window level: 50 HU, window width: 350 HU).

DATASET

| | |
|----------------|---|
| Name | Coltea-Lung-CT |
| #samples | 100 paired 3D CT volumes |
| Input Modality | Native (Non-Contrast) |
| Target | Arterial (Contrast-Enhanced) |
| Train/Test/Val | 75/15/15 CT volumes |
| Resolution | 256 × 256 × 96 voxels |
| Preprocessing | clip [-1000 HU, 1000 HU], normalize [0,1] |

INFERENCE STRATEGY

- 2D slice-wise inference with velocity aggregation for 3D consistency.
- Neighboring-slice averaging for drift correction.

KEY ADVANTAGES

- ✓ 100 training steps
- ✓ 3 inference steps
- ✓ 17.04s inference time per volume inference on H100 GPU.
- ✓ deterministic and reproducible output.
- ✓ improved structural consistency.

REFERENCES

- [1] Shiri et al., Slice-consistent BBDM for chest CT, 2025.
- [2] Ho et al., DDPM, NeurIPS 2020.
- [3] Isola et al., Pix2Pix, CVPR 2017.
- [4] Liu et al., Rectified Flow, ICLR 2023.

CONTACTS



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